Synthesis of calcium-deficient hydroxyapatite nanowires and nanotubes performed by template-assisted electrodeposition

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ARTICLE INFO

Keywords:
Electrodeposition
Calcium deficient hydroxyapatite
Nanowires
Nanotubes
Template synthesis

ABSTRACT

Hydroxyapatite (HA) has received much interest for being used as bone substitutes because of its similarity with bioapatites. In form of nanowires or nanotubes, HA would offer more advantages such as better biological and mechanical properties than conventional particles (spherical). To date, no study had allowed the isolated nanowires production with simultaneously well-controlled morphology and size, narrow size distribution and high aspect ratio (length on diameter ratio). So, it is impossible to determine exactly the real impact of particles’ size and aspect ratio on healing responses of bone substitutes and characteristics of these ones; their biological and mechanical effects can never be reproducible. By the template-assisted pulsed electrodeposition method, we have for the first time succeeded to obtain such calcium-deficient hydroxyapatite (CDHA) particles in aqueous baths with hydrogen peroxide by both applying pulsed current density and pulsed potential in cathodic electrodeposition. After determining the best conditions for CDHA synthesis on gold substrate in thin films by X-ray diffraction (XRD) and Energy dispersive X-ray spectroscopy (EDX), we have transferred those conditions to the nanowires and nanotubes synthesis with high aspect ratio going until 71 and 25 respectively. Polycrystalline CDHA nanowires and nanotubes were characterized by Scanning electron microscopy (SEM) and Transmission electron microscopy (TEM). At the same time, this study enabled to understand the mechanism of nanopores filling in gold covered polycarbonate membrane: here a preferential nucleation on gold in membranes with 100 and 200 nm nanopores diameters forming nanowires whereas a preferential and randomly nucleation on nanopores walls in membranes with 400 nm nanopores diameter forming nanotubes.

1. Introduction

Hydroxyapatite (Ca10(PO4)6(OH)2, HA), with a Ca/P ratio of 1.67, has attracted much attention because of its chemical and structural similarities with the key mineral component of human bone and teeth. HA is the thermodynamically most stable [1], the densest and the least soluble calcium phosphate (CaP). Due to its excellent biocompatibility, bioactivity, osteoconductivity and high compressive strength, HA and derivates are largely used in orthopaedic, dental and maxillofacial applications such as bone substitutes. But bone is constituted of nano-crystalline, non-stoichiometric, calcium-deficient apatites generally described by the following formula Ca10-x(PO4)6-x (HPO4)x(OH)2-x, [2] whose Ca/P molar ratio can go from 1.33 up to 1.67 [3]. Because of a lower Ca/P ratio than HA, calcium-deficient hydroxyapatite (CDHA) benefits from a higher solubility and consequently it biologically appears more bioactive than HA [4,5]. So CDHA, whose composition and structure are very close to the natural bone mineral, is of greater biological interest [6] than stoichiometric HA and a suitable candidate for bone regeneration [7].

Biological and mechanical properties of calcium phosphates are affected by the size, morphology, composition and structure of the particles. CaP nanoceramics, whose progresses in nanotechnology have allowed their fabrication since 1994 [8], are hopeful of becoming a new generation of bone substitutes. The scientific efforts made in
development of novel CaP formulations should lead to improved biomaterials, more suitable and effective for various biomedical applications. CaP materials can be used to reinforce polymer matrices and bone cements, porous 3D scaffolds for bone tissue engineering or for drug delivery. Because of their restricted size, high specific surface area, multiadsorbing sites and more favourable surface topography, nanoparticles [9] and particularly one-dimensional (1D) nanostructures such as nanorods, nanotubes [10], nanowires and nanowhiskers [11] have recently attracted much interest owing to their unique and remarkable properties (high aspect ratio, preferable biocompatibility, higher solubility, enhanced biological [9,12–14] and mechanical properties [15,16]...) and their potential use in many applications. Nanoparticles [9,12] and nanophase ceramics [18] can selectively and easier adsorb more specific proteins, enhance the adhesion and proliferation of osteoblasts, increase osteoblastic functions resulting in higher osteoconductivity and bioactivity than conventional particles and microphases ceramics. The integration of CaP nanowires [19] or nanotubes [17] is expected to enhance composites’ properties and mechanical strengthening. Therefore, such materials are excellent candidates for scaffolds in bone tissue engineering and bone substitutes [20].

HA nanofibers, nanowires or nanotubes have been produced by different methods such as hydrothermal process (the most useful method) [21], solvothermal process [22], or hydrothermal and sol-gel associated methods [23], nevertheless the majority of these methods enabled to obtain HA nanowires with a too wide size distribution [23–25], irregular and non-controlled morphology with an average aspect ratio (length on diameter ratio) limited to 30–50 [26–28]. This introduces major disadvantages: it is impossible to determine exactly the real impact of particle’s size and aspect ratio on healing responses of composite bone substitutes and their inconstant parameters forbid any reproducibility of the results. To date, no study had allowed the isolated nanowires production with well-controlled morphology and size and high aspect ratio by the template-assisted electrodeposition method.

The template method could be the only way to produce particles whose structure, morphology, size and array are well controlled. The use of the template method, for assisting metallic wires synthesis, was related by Bean in 1969 for the first time [29], followed by Possin by means of a porous etched mica and electroplating method [30]. Masuda and Fukuda were the first to report, in 1995, an ordered pores arrangement in anodic aluminium oxide membrane [31]. Then researchers used track-etched polycarbonate membranes [32].

Our study is the first that presents the synthesis of CDHA nanowires and nanotubes by using a template-assisted electrodeposition, with the exception of a study from Wang et al. who realized a highly ordered HA nanowires array (about 200 nm in diameter and 1 μm in length) and low aspect ratio of 5 [32]. Our method based on a pulsed electrodeposition with a recovering of nanowires separately should enable us to achieve much higher aspect ratios. Electrochemical deposition (ECD): one of the most common methods, offers many advantages such as low processing temperatures, a fast growth rate, a uniform deposition on irregular shapes and low cost. The quality of the deposits can be optimized by controlling the deposition parameters [33]. Recent studies have shown that coatings obtained by pulsed electrodeposition in presence of hydrogen peroxide (H2O2) showed less holes and craters, more uniformity, better adhesion and better mechanical properties than coatings produced with a constant potential [34]. It was also described that pulsed deposition allowed the growth of smaller crystallites than continuous deposition usually did and we hypothesized that it favoured nanowires formation.

The final objective of this work was to synthesize HA nanowires (or nanotubes) of very high aspect ratios with a regular and controlled morphology while offering a selection of 1D nanostructures with different diameters for several applications. In order to define the best parameters of the electrodeposition, we started by testing the electrodeposition in thin films on gold covered disks, using many deposition parameters and analysing the results. Our hypothesis is that the best parameters used in thin layers deposits should be similar to those we should use for the template method.

The present work presents the analysis by X-ray diffraction of these powders obtained from thin films crushing before and after a heat treatment at 850 °C, which enabled us to certify the exclusive presence of CDHA as crystalline phase. Finally, the optimized parameters for HA electrodeposition were transposed to the template method for elaborating high aspect ratio nanowires and nanotubes. Their characterizations were undertaken by Scanning electron microscopy and Transmission electron microscopy.

2. Materials and methods

2.1. Electrolyte preparation

The aqueous electrolyte bath was similar to the first one proposed by Shirkhanzadeh et al. in 1994: 0.042 mol.L−1 of Ca(NO3)2 and 0.025 mol.L−1 of NH4(H2PO4) were dissolved at room temperature in deionised water with a Ca/P ratio of 1.67 corresponding to the stoichiometric HA [8]. 0, 6 and 9 vol.% H2O2 were added in the bath in order to prevent hydrogen bubbles formation during electrodeposition and to favour a better calcium phosphate crystals nucleation [34,35]. H2O2 makes able to obtain different calcium phosphates; its concentration modifies the pH value of the bath. This one was adjusted to 4.5 or 6.0 by adding NaOH [33,36]. A forced convection was applied by using a peristaltic pump, in order to prevent settling, for keeping a stable composition of the bath around the cathode and for pumping hydrogen bubbles that can get into nanopores and alter the composition and structure of the synthesized material. Bath stirring was also reported helpful for obtaining CaP crystals in nanosize [37].

2.2. Electrodes preparation

Experiments were performed in a three-electrode cell. Pt wire acts as the auxiliary electrode; before using, it was cleaned with 99.9% alcohol then heated in a hydrogen flame till red glow. An Ag/AgCl electrode was used as the reference electrode. The working electrodes were firstly stainless steel disks, then once the electrodeposition parameters selected, track-etched polycarbonate membranes were used as cathodes. The disks were mechanically polished with increasingly finer grades of SiC paper, rinsed with alcohol 99.9% and dried. Then, they were covered with a 300 nm gold film by a physical vapor deposition process. The gold covered disks active surface area for the deposits was 0.125 cm². For the nanowires synthesis, Whatman® Cytoclear nuclear track-etched polycarbonate membranes were used as a template. Three references of membranes have been used (100, 200 and 400 nm pore diameters) with 11 μm nominal thickness. One side of the membrane was coated by sputtering with a 300 nm gold film. This conductive film acts as the cathode. The pores densities quoted by the supplier and the active surface area (total area of the pores) were respectively 6.10⁵/cm² and 5.89.10⁻² cm² for membranes with pores of 100 nm diameter, 5.10⁴/cm² and 1.96.10⁻² cm² for membranes with pores of 200 nm diameter and 1.5.10⁵/cm² and 2.38.10⁻² cm² for membranes with 400 nm pores diameter. The horizontal upward working electrode was connected to the potentiostat.

2.3. Experimental setup

The cathodic electrodeposition was conducted in an electrochemical cell made of glass with a polymer covering (Fig. 1a). The three electrodes were immerged in an electrolytic bath whose temperature was maintained at 70 °C using a hot water flow in a double-wall electrochemical cell [38]. In the sample holder made of polymer, the stainless steel disks and membrane disks were maintained between a join and a screw. A stainless steel grid was interposed between the cathode and the disks. The distance between counter and cathodic electrodes was
fixed at 20 mm. The reference electrode (Ag/AgCl) was maintained in proximity to the cathode.

### 2.4. Electrodeposition

The cathodic depositions were carried out under a vertical laminar flow hood with a Radiometer PGZ301 Potentiostats controlled by VoltaMaster4 software operating in static and pulsed mode. Before deposition, the membranes were placed into the electrolytic bath for 4 min so as to impregnate them with it.

Preliminary cyclic voltammetry (CV) experiments were carried out on a gold covered stainless steel disk at 70 °C and conducted at a scan rate of 10 mV/s (Fig. 2). The electrodeposition was performed at 70 °C in a potentiostatic or intentiostatic mode. The effective period of deposition was 3 min, 5 min [39], 10 min and 15 min. The final chosen value of effective potential was −1.6 V/Ag/AgCl according to other studies [8]. The values of current density applied for thin films in constant mode (−15 and −20 mA·cm⁻²) were chosen in accordance with works which succeeded to electrodoposit HA [34,39,40]. Deposition in membrane was successful only for higher values of current density [40–42], so an effective value of −120/−250 mA·cm⁻² was applied correspondingly to the average values registered during a potential imposition of −1.6 V/Ag/AgCl [43]. Electrodeposition was firstly carried out in constant mode and then in pulsed mode (Fig. 1b). The conditions of pulsed electrodeposition were those chosen by Drevet et al. [34]; five deposition cycles were imposed, each one was composed by a deposition time (60 s; E = −1.6 V/Ag/AgCl or I = −120 or −150 mA·cm⁻²), followed by a break time (120 s; value of free potential or 0 mA·cm⁻² respectively). Some deposits were realized by alternating 1 s deposition time and 2 s break time such as metallic nanowires produced in others studies [44]. A low frequency pulse was chosen to give the system time to recover during the off period. Chrono-potentiometric and chrono-amperometric curves were followed (Fig. 1b).

### 2.5. Thin films and nanowires/nanotubes characterisation

Thin films obtained were characterized by a Bruker Analytical D8 Advance X-ray diffractometer operating with a Cu Kα radiation (λ = 1.5418 Å) at 40 kV and 40 mA, in the 0-θ mode. X-ray patterns data (Fig. 3’ and 3”) were collected in the 20 range between 3 and 70°, with a 20 step of 0.04°, a counting time of 2 s by step and a 30 rpm for spinning speed of the sample holder. The chemical composition of thin films (Ca/P molar ratios) was investigated by energy dispersive X-ray spectroscopy (EDX). SEM analysis was performed using a JSM-6460LA microscope (Jeol) operating at 13 kV and results of the Ca/P atomic

<table>
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<th>Samples</th>
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<th>pH</th>
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<td>Constant</td>
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<td>Constant</td>
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<td>c</td>
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<td>6.0</td>
<td>−80/−110</td>
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</tr>
<tr>
<td>d</td>
<td>9</td>
<td>4.8</td>
<td>−50/−75</td>
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<tr>
<td>g</td>
<td>9</td>
<td>6.0</td>
<td>−80/−115</td>
<td>Constant</td>
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<tr>
<td>h</td>
<td>9</td>
<td>6.0</td>
<td>−65/−90</td>
<td>Pulsed</td>
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</table>
ratio were reported as the mean of measurements.

In order to differentiate HA and OCP, a heat treatment of the calcium phosphate powders obtained by thin films crushing have been done such as Karampas et al. works [45]. The deposits were subjected to a temperature of 850 °C under N₂ flow, during 2 h after an increasing and before a decreasing in temperature of 10 °C/min. X-ray powder diffraction (XRPD) analysis of the crystal structure and Ca-P phases identification of the synthesized powders were performed before and after heat treatment (Fig. 3').

After electrodeposition, for collecting the nanowires (Fig. 1c), the membranes were rinsed with deionised water, air dried then dissolved with dichloromethane heated at 40 °C [46] until being dried. The size and morphology of nanowires/nanotubes were investigated by scanning electron microscopy (SEM). SEM analysis was performed using the JSM-6460LA microscope (Jeol). A Transmission electron microscopy (TEM) was performed at 300 kV using a H9000NAR microscope from Hitachi (Scherzer resolution 0.18 nm); TEM images and selected-area electron diffraction (SAED) patterns were performed to study and confirm the structure and morphology of nanowires at the nanometer scale.

3. Results

Firstly, the cathodic part of cyclic voltammogram (Fig. 2) with a stabilization of the current density between −1.5 V and −2.2 V/Ag/AgCl enabled to confirm the electrochemical potentials window (corresponding to the diffusion level) allowing the HA electrodeposition with minimized secondary compounds formation between those two values. So, the desired potential range for HA electrodeposition may be comprised between −1,5 and −2,2 V/Ag/AgCl before the hydrogen evolution reaction becomes dominant [47], indicated by a sharp increase in the cathodic current density beyond −2.2 V/Ag/AgCl [47,48]. By varying the deposition parameters (Table 1), we obtained different thin films. Those films were submitted to an X-ray diffraction...
analysis. The XRD patterns (Fig. 3a, 3c) showed diffraction peaks characteristic of gold at \(2\theta = 38.16^\circ, 44.38^\circ\) and 64.56° and corresponding to the substrate (gold coating on the disks) and close to 8.10°, 18.75° and 34.58° attributed to the stainless steel disks and adhesive band (stabilizing the disks). The identification of the other peaks was difficult because many calcium phosphates give two theta diffraction peaks in very close position. In absence of \(\text{H}_2\text{O}_2\) (Fig. 3a), only the substrate gave peaks with no identified calcium phosphates. In presence of 6 and 9% vol \(\text{H}_2\text{O}_2\), calcium phosphates were detected. At pH 4.5, a peak at 11.70°, identified as (020) plane of brushite (DCPD, CaHPO4·2H2O, ICDD file n° 009-0077) and one of the two more intense peaks of its XRD pattern could be seen in constant potentiostatic mode (Fig. 3d, 3e) but absent in pulsed potential mode (Fig. 3f). At pH 6.0, whether constant or pulsed mode, no peak at 11.7° was present (Fig. 3a, b, c, 3g, h). All other diffraction peaks could be assigned to HA or OCP according to the standard database respectively ICDD file n° 009-0432 and ICDD file n° 079-0423 or to CDHA; their X-ray patterns, very similar may be confused. XRD patterns show broad and small peaks, larger at pH 4.5 (Fig. 3d) than at pH 6.0 (Fig. 3e). The peaks are narrower and have a higher intensity in pulsed mode compared to constant mode for films deposited at pH 4.5 (Fig. 3f > c), and at pH 6.0 (Fig. 3h > g) in the studied potentiostatic mode. It was the same observations by applying a current density (data non presented).

Finally, in the best conditions for obtaining HA deposits, we may have synthesized HA, CDHA, OCP or a mix of these phases. The strongest peaks were identified, their position at about 25.9°, 31.8°, 32.2° and 32.9° correspond respectively to the (002), (211), (112) and (300) planes of HA or could correspond to peaks of OCP. Without \(\text{H}_2\text{O}_2\) thin films (Fig. 3a) were usually difficult to obtain, so no Ca/P molar ratio could correctly be measured. The Ca/P molar ratios of thin films (Fig. 3f) were comprised between 1.46 and 1.74. Thin films obtained at pH 4.5 (Fig. 3e) or 4.8 (Fig. 3d) with 9% vol \(\text{H}_2\text{O}_2\) in constant mode were associated to a Ca/P ratio of 1.46. At pH 4.5 with 9% vol \(\text{H}_2\text{O}_2\) but in pulsed mode Ca/P ratio was 1.52 (Fig. 3f). At pH 6.0, with 6% vol \(\text{H}_2\text{O}_2\) in constant mode the Ca/P molar ratio was 1.53 (Fig. 3b) and with 9% vol \(\text{H}_2\text{O}_2\) in constant mode, the Ca/P molar ratios were 1.57 and 1.74 in constant mode for the 2 different samples realized in the same conditions (respectively Fig. 3c and 3g). In summary, in the best conditions, at pH 6.0 with 9% vol \(\text{H}_2\text{O}_2\) and pulsed mode (Fig. 3h) the Ca/P molar ratio was 1.55.

Powders, obtained from the crushing of thin films obtained in the best conditions of HA electrodeposition (pH 6.0, 9% \(\text{H}_2\text{O}_2\), pulsed mode (with \(t_{\text{on}} = 1\) min at \(E = -1.6\,\text{V}_{\text{Ag/AgCl}}\) and \(t_{\text{off}} = 2\) min at \(E = \text{free potential}\) for a 15 min effective deposition time) were submitted to an X-ray diffraction analysis for identifying the electrodeposited materials. The obtained XRD patterns (Fig. 3g) showed diffraction peaks at \(2\theta = 38.16^\circ, 44.38^\circ\) and 64.56° characteristic of gold from the deposited layer. All other diffraction peaks could be assigned to HA (or CDHA) compound with absence of OCP owing to that the most intense characteristic (001) diffraction peak at \(2\theta = 4.74^\circ\) was not observed, respectively to the PDF database files JCPDS 009-0432 and JCPDS 079-0423 of these HA and OCP compounds. So, the XRD patterns revealed that the deposits were composed of HA or CDHA. The X-ray diffraction patterns of powders (XRPD) showed the typical peaks of HA/CDHA; the strongest peaks were found at about \(2\theta = 10.82^\circ, 25.88^\circ, 31.77^\circ, 32.19^\circ\) and 32.90° corresponding respectively to the diffraction on the (100), (0 0 2), (2 1 1), (1 1 2) and (3 0 0) crystallographic planes of HA (Fig. 3h).

In order to confirm the absence of OCP, we have submitted to an annealing (850 °C 2 h - N2 flow), the powders issued from the crushing of thin films, based on Karampas et al. works [45,49]. After heat treatment, the XRD spectra (Fig. 3h) revealed, the intense peaks of 3 phases: gold (coming from the sputtered gold coating weakly adhering to the stainless steel disks), HA and \(\beta\)-TCP whose six more intense peaks not assignable to HA are at \(2\theta = 13.56^\circ, 27.75^\circ, 30.98^\circ, 34.30^\circ, 46.91^\circ\) and 52.99° (JCPDS 09-0169).

Before starting the template method, we controlled the thickness for one non-deposited polycarbonate membrane with 200 nm pores diameter on a cross sectional SEM view of this one (Fig. 4a) The measured value was 15.5 μm which allowed us to suppose that the 11 μm nominal thickness indicated by the society was not correct or inhomogeneous.

Although pulsed deposition produced the thickest and a more uniform coating in thin film, deposition in polycarbonate membrane occurred mostly at the periphery of the substrate rather than in its center (Fig. 4a). Moreover, we often observed a rupture of the membranes in this peripheral zone (Fig. 4a) and an inflation (Fig. 4b). A metallic grid was interposed between the gold covered membrane (cathode) and the stainless steel disk cathode, in order to improve the electrical contact. With this grid, we have extended the deposition to all the membrane surface (Fig. 4c) and prevented the membrane to break and to inflate as observed by optic microscopy (Fig. 4d).

SEM micrographs showed that the 300 nm thickness gold coating evaporated on any membrane left the pores open (whatever its nanopores diameter) (Fig. 5a). Gold layer entered the first nanometers of pores and deposited on the nanopores walls without closing them completely as seen on SEM micrographs (Fig. 5b). Imperfect (because of porous walls) nanotubes (Fig. 5c, f) have been synthesized at \(-1.6\,\text{V}_{\text{Ag/AgCl}}\) respectively from membranes with 100 nm pores diameter (Fig. 5d, f) and 400 nm pores diameter (Fig. 5e) in pulsed mode (15 min effective deposition time, deposition time 1 s, break time 2 s). Nanotubes and nanowires could also be simultaneously synthesized as it could be seen from a sample with a deposition carried out in constant mode during 30 min at \(-1.6\,\text{V}_{\text{Ag/AgCl}}\) (Fig. 5e).

Nanowires, obtained with the three different membranes, were observed by SEM on silicon wafer after membrane dissolution. The micrographs (Table 2) showed heaps of nanowires viewed on their length. The presented nanowires were produced by pulsed potential \((-1.6\,\text{V}_{\text{Ag/AgCl}}\) in membrane with pores diameter of 100, 200 and 400 nm during different time.

With the 100 nm pore size polycarbonate membrane, the aspect
ratio of nanowires (diameter/length ratio) were in the range of 20 to 43 for 3 min and 37 to 71 for 5 min effective deposition duration with a final diameter comprised between 220 and 350 nm going until 3.5 times higher than original pores diameter. The aspect ratios of nanowires obtained in 200 nm pore size polycarbonate membranes were in the range of 19 to 22 for 5 min' deposition time and 21 to 53 for an effective 15 minutes' deposition time. Their diameters measured 270 or 370 nm, i.e. until 1.8 times the original pores diameter. Others nanowires, obtained in membranes with a 400 nm pore diameter, presented an aspect ratio comprised between 10 and 19 for 5 min and between 9 and 25 for 15 min effective deposition time. Their average diameters started from 590 to 970 nm corresponding to a nanopores expansion going from 1.5 to 2.4 times.

The nanowires observed by TEM were obtained in the best conditions of synthesis (pH 6.0, 9% H2O2 and pulsed mode with tON = 1 min and tOFF = 2 min) with pulsed potential at −1.6 V/Ag/AgCl (Fig. 6) and pulsed current density at −120 mA/cm2 (Fig. 7) in a membrane whose pores diameter was 200 nm and with pulsed potential in a membrane with 400 nm pores diameter (Fig. 8). The TEM micrographs of the nanowires (constituted of nanoneedles) are presented (Figs. 6a, b, 7a, b, 8a and b) with the related selected area electron diffraction (SAED) patterns (Figs. 6d3, d4, 7d1", d2 and 8d3".*). Those patterns present two intense partial rings of electron diffraction spots with distances of 0.33 nm and 0.27 nm corresponding respectively to the diffraction on (0 0 2) and (2 1 1) crystal planes of an apatite-like structure. The observation at high magnification (Figs. 6V3-60K, V3-400K, 7V1-500K, **Fig. 5.** SEM micrographs: a) porous gold covering on a membrane with 100 nm nanopores diameter and 300 nm gold thickness; b) cross sectional view of gold coated polycarbonate membrane with 200 nm nanopores diameter; c) porous nanotubes obtained from 400 nm pores diameter membrane in pulsed mode (15 min effective deposition time, deposition time 1 s, break time 2 s); d) nanotubes seen from one tip, in membranes with 100 nm nanopores diameter; obtained in pulsed mode (15 min effective deposition time, deposition time 1 s, break time 2 s) e) nanotubes and nanowires synthesized from deposition in constant mode during 30 min at −1.6 V/Ag/AgCl in membranes with 100 nm nanopores diameter; f) porous nanowires obtained from 100 nm pores diameter membranes in pulsed mode (15 min effective deposition time, deposition time 1 s, break time 2 s).

Table 2

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<th>Membrane pores diameters</th>
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Experiments concerning the mechanical or biological properties of these nanowires that we produced could give us hope that future exploitation could thus be optimized for many applications and the homogeneity of diameter and density of nanopores. The performance of HA particles in the choice of the membrane characteristics: respectively thickness, porosity, morphology. Nanowires length, diameter and amount can be modulated by the electrodeposition; this template method involved the synthesis within the pores of a nanoporous membrane. The advantage of the template electrodeposition; this template method is based upon nanowires being generally the exact replica of the pores of a nanoporous membrane. The advantage of the template method would be too limited to perform physicochemical analyses, the optimal depositional conditions were determined by the deposition of thin films on gold obtaining a sufficient quantity for its characterization and keeping the same electrochemical conditions. The deposits (in thin films and membranes) have been performed at a temperature of 70 °C based on many works that have demonstrated crystalline HA formation at a temperature comprised between 60 °C [35,53] and 85 °C [54]. Electrolyte pH affects also directly the nature and crystals size of CaP phases [42]; Montero et al. highlighted that crystals size decrease with increasing pH for reaching a nanometer size at pH 6. In mostly studies [33,36], deposition in acid baths, with pH range from 4 to 6, favours OCP formation with less crystallized deposition. Its nucleation and growth would be kinetically more favourable under physiological conditions [1]. But the more the pH reaches a weak acidic value between 6 and 7.4, the more HA is present until being the only phase [33,36]. So, usually a higher pH favours monophase and nanocrystals HA formation [33,36] but electrodeposition often results in deposition of other calcium phosphates: OCP, β-TCP (β-Ca3(PO4)2, whitlockite) or DCPD (CaHPO4·2H2O, brushite) more probably because of lower pH generated at the cathode. In our bath, with adding NaOH for increasing the pH, an intense precipitation occurred which can disturb electrodeposition in nanopores. A compromise was found by choosing a weak acidic solution with an effective pH 6.0, sufficiently high to enable alone HA formation and not too high to prevent an important precipitation before electrodeposition.

The nanowires were produced in this study by a template-assisted electrodeposition; this template method involved the synthesis within the pores of a nanoporous membrane. The advantage of the template method is based upon nanowires being generally the exact replica of nanopores in diameter and length in a polycarbonate membrane. This method is consistent with the Fourier Transform of a squared area of one nanoneedle (Fig. 7FT) is periodicity of 0.34 nm along the longitudinal axis (Figs. 6V3-400K, 7V1-500K and 8V3-400k) and 0.82 nm along a transversal axis (Figs. 7V1-400K and 8V3-400k) of the nanoneedles which are respectively consistent with the [001] and [100] directions of HA. Moreover, the Fourier Transform of a squared area of one nanoneedle (Fig. 7FT) is consistent with the simulated electron diffraction pattern of HA structure along the [010] zone axis (Fig. 7SEDPA).

We can observe on TEM micrographs at moderate magnification the opacity of 1D structures obtained from membranes with 200 nm pores diameter (Figs. 6a, b, 7a, b) and the transparency of 1D structures obtained from membranes with 400 nm pores diameter (Fig. 8a, b). The nanoneedles constituting the 1D structures from membranes with 200 nm pores diameter were roughly uniaxially oriented in the longitudinal axis of nanowires (Figs. 6a, V3-60k, 7a) whereas nanoneedles constituting 1D structures from membranes with 400 nm pores diameter were multiaxially oriented (Fig. 8a, b).

4. Discussion

The nanowires were produced in this study by a template-assisted electrodeposition; this template method involved the synthesis within the pores of a nanoporous membrane. The advantage of the template method is based upon nanowires being generally the exact replica of nanopores in diameter and length in a polycarbonate membrane. This nanowires synthesis never realized before makes possible a fast production of calibrated nanowires with a predetermined size and morphology. Nanowires length, diameter and amount can be modulated by the choice of the membrane characteristics: respectively thickness, diameter and density of nanopores. The performance of HA particles could thus be optimized for many applications and the homogeneity of the nanowires that we produced could give us hope that future experiments concerning the mechanical or biological properties of these compounds will be reproducible.

Our study is the first in which CaP nanowires are produced by pulsed electrodeposition in polycarbonate membranes. It is the second study applying a pulsed potential for a CaP electrodeposition [35] and the third time that calcium phosphates are electrodeposited on gold substrate [50,51]. This synthesis employed aqueous baths, ensuring toxicity-free produced compounds, developed by Shirkhanzadeh et al. who succeeded, as early as 1991, to produce CaP deposits by electrodeposition [52]; in our work, hydrogen peroxide has been added.

Knowing that the quantity of nanowires produced by the template method would be too limited to perform physicochemical analyses, the optimal depositional conditions were determined by the deposition of thin films on gold obtaining a sufficient quantity for its characterization and keeping the same electrochemical conditions.

The deposits (in thin films and membranes) have been performed at a temperature of 70 °C based on many works that have demonstrated crystalline HA formation at a temperature comprised between 60 °C [35,53] and 85 °C [54]. Electrolyte pH affects also directly the nature and crystals size of CaP phases [42]; Montero et al. highlighted that crystals size decrease with increasing pH for reaching a nanometer size at pH 6. In mostly studies [33,36], deposition in acid baths, with pH range from 4 to 6, favours OCP formation with less crystallized deposition. Its nucleation and growth would be kinetically more favourable under physiological conditions [1]. But the more the pH reaches a weak acidic value between 6 and 7.4, the more HA is present until being the only phase [33,36]. So, usually a higher pH favours monophase and nanocrystals HA formation [33,36] but electrodeposition often results in deposition of other calcium phosphates: OCP, β-TCP (β-Ca3(PO4)2, whitlockite) or DCPD (CaHPO4·2H2O, brushite) more probably because of lower pH generated at the cathode. In our bath, with adding NaOH for increasing the pH, an intense precipitation occurred which can disturb electrodeposition in nanopores. A compromise was found by choosing a weak acidic solution with an effective pH 6.0, sufficiently high to enable alone HA formation and not too high to prevent an important precipitation before electrodeposition.
In this work, at pH 4.5 and constant mode, brushite formation was favoured; one of its two intense XRD peaks at 2 theta = 11.7° was identified in the two samples obtained in this condition (Fig. 3d and 3e). With a Ca/P ratio of 1.0 for brushite and a Ca/P ratio of 1.67 for stoechiometric HA, the Ca/P molar ratio of 1.46 for this two samples (Fig. 3d and 3e) corroborates the presence of brushite together with HA. Whereas at pH 6.0, all XRD peaks found were identified as HA or CDHA peaks (Fig. 3b, 3c, 3g, 3h, 3i).

In aqueous baths, the cathodic reduction of water, dissolved oxygen and phosphates groups results in a local and fast pH increase at the cathode’s surface due to the generation of OH ions, inducing a nucleation on the cathode. But the electrochemical deposition has the disadvantage to generate H2 bubbles that start evolving from the cathode surface [35,39], lead to the formation of volcano structures [54] and can prevent further CaP deposition (nucleation and growth). Our study, confirming partially the conclusion of many authors [34,39], revealed a better CaP deposition in presence of 6–9% vol H2O2 (Fig. 3b, c, d) and the best with pulsed mode (Fig. 3h); the obtained thin films were composed of CDHA. In some studies, the addition of 9% H2O2 could even lead to monophasic HA instead of CDHA with 6% H2O2 [34,39]. Hydrogen peroxide (H2O2), recognized preventing bubbles formation (and/or favouring ions OH− production), has the advantage to increase the pH leading to the predominant formation of the HA phase.

CDHA thin films after pulsed deposition [34,35,39] were previously found more crystallized, more uniform, denser and more adherent compared to their counterpart obtained in intenstionic constant modes. LeGeros [55] was able to deposit CDA directly by pulsed ECD and in many studies, pulsed ECD associated with H2O2 leads to dense and uniform monophasic HA coatings [35,39]. In pulsed mode, the relaxation time between two deposition times strongly reduces H2 bubble emission and gives the calcium and phosphate ions in the solution sufficient time to diffuse to the cathode surface [34,56]. The generated hydrogen may have time to escape [48]. Our XRD analyses (Fig. 3) showed that electrodeposited coatings in pulsed mode were composed of a CaP phase with typical diffraction peaks corresponding to HA/CDHA apatite-like structure (JCPDS 09-0432) (Fig. 2). It has also been described by many authors that pulse deposition gives rise to smaller crystallites (HA nanoparticles) than continuous deposition does [56]. This factor logically favours the nanowires formation.

So, in this work, benefits of 6–9% H2O2, pH 6.0 and pulsed mode, enabling the exclusive formation of HA (and/or OCP) in more homogeneous and denser deposits, were confirmed in thin films by XRD analyses (Fig. 3h). These conditions have generated narrower and
higher XRD peaks than others conditions (0% H2O2, pH 4.5 and constant mode) did (Fig. 3), confirming a higher crystallinity and/or a higher amount of these deposits. Those observations explained why in the present study, pulsed electrodeposition and an optimal quantity of H2O2 in electrolyte were combined for the nanowire synthesis.

XRD patterns of our thin films were more in favour of a hydroxyapatite or a calcium-deficient hydroxyapatite but XRD peaks that remain wide and with low intensity could also testify the presence of nanocrystals or HA films with low crystallinity. There is also a possibility of misidentification between OCP and HA when using only the X-ray diffraction analysis at high angle (20 > 10°) because of their similarity in structure [57]. There is an extended overlapping between the peaks of OCP and HA especially in the region 25° and 31° where the peaks are of higher intensity corresponding respectively to the (002) plane and a combination of the (211), (112) and (300) planes of HA [49]. The main difference that may be able to distinguish OCP from HA is the most intense characteristic diffraction peak of OCP at 20 = 47° corresponding to the diffraction by the (100) crystallographic plane and additionally its two diffraction peaks at 20 = 9.4° and 9.8° corresponding respectively to the diffraction by the (110) and (010) planes of its structure (according to the PDF file JCPDS 079-0423) that we have never observed [33,36] (Fig. 3). A reason for explaining why these peaks could be too small for being observed, could come from a highly textured coating with a particular crystalline orientation or could also be hidden by the background; but after crushing thin films in powders, no peak at 4.7°, 9.4° and 9.8° were detected (Fig. 3”) that was in favour of the absence of OCP. Distinction between CDHA and HA nanocrystals [3] is also complicated with lower and broader XRD peaks than those of stoichiometric HA. Pulsed mode at pH 6.0 with 9% vol H2O2 gave the best results in terms of composition, crystallinity and amount of deposition but our methods of characterization (analyses by XRD (Fig. 3)), Raman and Infra-red spectroscopies) appeared to be insufficient to determine the exact composition of the electrodeposited materials. In the SAED patterns (Figs. 6, 7 and 8), although OCP presents, at low diffraction angle, intense reflection corresponding to the diffraction by the (100) plane at distance of 1.9 nm that makes able to clearly distinguish OCP from HA, it was not possible to observe this diffraction spot because of its absence or especially because of the occultation by the beam-stop and the highly intense spot of the direct beam which make it difficult to observe.

There was the same problem of peaks overlapping in the X-ray diffractograms and in Infra-red or Raman spectra for thin films. A method described by Karampas et al. was transposed to our samples [45]. The CaP powders obtained by crushing two thin films obtained after 15 min effective deposition time (realized in the best and the same conditions than for nanowires) were submitted to a heat treatment, at 850 °C during 2 h, in order to determine OCP presence (Fig. 3”). It is well accepted that stoichiometric HA heat treated up to 1200 °C keeps its crystallographic structure [45,58] because it’s the most thermodynamically stable CaP phase; on the contrary, the instable OCP converts into β-TCP (beta tricalcium phosphate, JCPDS 09-0169) and β-CPP (calcium pyrophosphate, β-Ca2P2O7, JCPDS 01-071-2123) [49]. Some studies have highlighted the transformation of poorly crystalline CDHA in a biphasic mixture of HA and β-TCP during calcination at temperature close to 800 °C [58,59]. After heat treatment, XRD analysis (Fig. 3”) revealed that powders were composed of three compounds: gold (coming from the gold film sputtered on stainless steel disks), HA and β-TCP identified by their characteristic peaks. Although the SAED patterns (Figs. 6, 7 and 8) could also be controversial for phase identification because their spacing values (0.34 and 0.28 nm) exist both in HA and OCP [60], the XRD analysis of the heat-treated powders indicating the absence of β-CPP and presence of β-TCP, coupled to the Ca/P ratio of 1.55 in the same conditions (pH 6.0, 9% vol H2O2 and pulsed mode) (Fig. 3”), enabled us to conclude on the absence of OCP and that the original thin films were composed of CDHA whose apatite-like structure was the only crystalline phase observed by TEM (Figs. 6, 7 and 8). So it could logically be thought that the composition of the nanowires is the same as that of thin films in the same electrochemical conditions. This confirms the description of other authors [3,36] saying that HA can be the only component in weak acidic conditions and the results of Lu who declared that the CDHA formation is favoured in aqueous solutions [1]. In our thin films, an amorphous phase (ACP), whose presence was suggested by a perturbated background on X-ray diffractograms [53,61], could explain Ca/P ratios higher than 1.67 (Fig. 3”) but some residues of Ca(OH)2 coming from reaction between OH- and Ca2+ ions could also explain it. The XRD peaks, generally broad, could be attributed to a poor crystallinity, residual strain [62] or a nanocrystalline structure [2].

A Rietveld refinement of the X-ray diffraction patterns of the heat-treated powders (obtained from crushing of thin films deposited during 15 min effective duration) was realized for a quantitative evaluation of composition. The fractions of β-TCP and HA found were very similar for the two conditions: 69.0 and 31.0% weight respectively in pulsed potentiostatic mode (−1.20 mA/cm2) and 69.5 and 30.5% weight respectively in pulsed potentiostatic mode (−1.6 V/Ag/AgCl). Many authors have remarked that the obtained compounds are dependent on the initial Ca/P ratios of the precursors and that HA/β-TCP ratio is determined by the initial calcium-deficiency and sintering temperature [63]. A higher proportion of β-TCP is indicative of an increased calcium deficiency of the original CDHA (before calcination) [64]. In parallel, the Ca/P ratio of the initial CDHA can be calculated by determining the phase proportions in the calcined biphasic materials and inversely the proportion of β-TCP/HA of the calcined compounds can be estimated from the Ca/P ratio of the non-heated powders [64]. With the help of the Rietveld Refinement, by knowing the ratio of HA/β-TCP, we could easily deduce the Ca/P ratio of the original thin films (before heat-treatment). This average composition gave an estimated value of the expected Ca/P ratio of the original thin films of 1.55 that corresponded very closely to the Ca/P ratios’ values of our thin films estimated by EDX spectroscopy (1.55 (Fig. 3”) and 1.52 in potentiostatic and potentiostatic modes respectively), enabling to corroborate the conclusions of the heat treatment saying that thin films were composed of CDHA whose Ca/P ratio (between 1.33 and 1.67) is smaller than the
theoretical value of stoichiometric HA (1.67). For memory, the Ca/P value of OCP is 1.33 and that of ACP ranges from 1.0 to 2.0. The absence of other elements (possible carbonates or sodium atoms) detected by spectroscopic studies enabled us to conclude that CDHA synthesized was not substituted.

These optimized conditions for synthesizing on gold a calcium-deficient hydroxyapatite (CDHA) in dense and homogeneous thin films were transferred to the nanowires synthesis on gold covered polycarbonate membranes.

Generally, an intensttiostatic mode is preferred instead of a potentiostatic mode because of a better deposition process control and generally denser and thicker deposits. Our results also corroborate the suggestion of Han et al. [65] saying that a high current density can increase ions quantity deposited with a competition of crystalline growth inducing a slower growth and explaining smaller crystals size [55] and a more dense and uniform structure. In many studies [61], OCP is obtained at weak current density and monophasic nanoparticles HA coatings at high current densities: between 50 and 240 mA/cm$^2$ [40-42] even if some authors have obtained HA with low current density (such as 1 mA/cm$^2$) [66]. It is recognized that applying a high current density during pulsed electrodeposition gives a greater cathodic potential ($> -2$ V$/$SCE) conducting to a favourable higher pH in the vicinity of the cathode. A potentiostatic mode was also tested because it is impossible to exactly determine the real active surface area of membranes. Because of H$_2$ bubbles progression into some pores, the surface area could be reduced and this gives to a non-determinated part of the membrane a non-conductivity.

It was remarked the best results in term of crystallinity, density, homogeneity and only presence of CDHA for a potential close to −1.6 mV/$/$AgAgCl. This potential value was chosen because of its localization inside the electrochemical potential window (Fig. 2). The current density registered for this potential was comprised between −65 and −90 mA/cm$^2$ for thin films (Table 1) whereas it was comprised between −120 and −300 mA/cm$^2$ for depositions in polycarbonate membranes (Table 2).

After electrodeposition, in agreement with Blackwood works on thin films [56], a more abundant deposition on polycarbonate membrane was mostly observed at the substrate periphery rather than at its center along with a distortion of the membranes (Fig. 4'$a$), possibly due to edge effects which generate also a greater hydrogen evolution. Hydrogen bubbles can pass through the porous and weak membranes and this can explain why we found the membranes inflated and ruptured all around the periphery resulting in isolation from the cathode (Fig. 4$^c$). Other reasons could be the impregnation of the membrane by the bath, the possible diffusion through the membrane of this one that inflates with temperature and the stresses exercised by a current applying. With a metallic grid interposed between the membrane and the cathode, the membrane doesn’t inflate (Fig. 4$^d$), the electrical contact is enhanced and the deposit obtained is more uniform (Fig. 4$c$); we have extended the deposition to the entire surface of the membrane and surely gained in quantity of nanowires.

Because the amount of produced nanowires was too low to be analysed by XRD, they were observed by SEM microscopy and a TEM analysis was realized for assessing the presence of apatite. The physical (shape, size and distribution of the pores) and chemical (composition and functional groups on surfaces) properties of the membranes are considered as the main factors for controlling the size and morphology of the products. The polycarbonate membranes contain cylindrical and non-connected nanopores, with mono-dispersed diameters, which extend through their entire thickness. After their dissolution in dichloromethane heated at 40 °C, nanowires could be distinctly observed on micrographs in Table 2 signifying the success of the template-assisted electrodeposition. The obtained HA nanowires had an almost uniform length and diameter.

The nanowires diameter is predetermined by the nanopores diameter and their length can be controlled by the duration of electrodeposition but the average length and diameter of the nanowires seen on SEM micrographs (Table 2) didn’t correspond exactly to those of nominal nanopores. We observed for all the membranes, an increasing length of nanostructures (nanowires/nanotubes) with deposition time (Table 2). The maximum length to obtain corresponded logically to the membrane thickness but the longest nanowires were curiously longer than expected as Zhang [67] could observe it with metallic nanowires. In our study, the longest produced nanowires measured 15.9, 14.5 and 15.6 μm for the membranes with 100, 200 and 400 nm nanopores diameters respectively suggesting that the membranes were thicker than the thickness value declared by the fabricant (11 μm) and were close to 16 μm. This hypothesis was most likely after the thickness measurement of 15.5 μm determined by SEM on membrane cross-sections (Fig. 4). The thickness of the membranes may also not be perfectly constant or owing to the random nature of the pore-production process, all pores may not be of the same length than the membrane thickness because the angle of the pores with respect to the surface could be as large as 34° [68]. This last hypothesis was refuted by the SEM observation of nanopores close perpendicular to the surface of the membrane in a cross-sectional view (Fig. 4$^b$). But some nanowires produced during the same duration, were shorter (Table 2). This could be explained by the explanation of Blackwood [56] with the fact that a constant deposition by potentiostatic method could be hard to control because as the dielectric Ca-P forms, a potential drop could occur leading to a decrease of the deposition rate during the experiment. By a mass transport limitation or an ohmic drop generated by the electrolyte, potential can also decrease and stop the nanowires growth. It could also be explained by a progression of H$_2$ bubbles that blocks the synthesis or because the nanowires randomly break as a result of the presence of defects and their intrinsic weakness [67]. With metallic nanowires, Keating stated that particles with aspect ratio above 25 are susceptible to breakage [69].

Finally, we observed (Table 2) the entire filling of nanopores after 5 and 15 min of effective deposition for membranes respectively with 100 and 200 nm nanopores diameters enabling to obtain nanowires with respective aspect ratios of 37 to 71 and 21 to 53. For membranes with a 400 nm pores diameter, 10 min enabled to obtain nanotubes with the maximal length close to 16 μm and an aspect ratio from 9 to 25. Increasing deposition time with this last membrane didn’t lead to the filling of nanotubes with nanowires formation but the weakness of the membranes after some time in electrolyte limited often proper observations.

The nanowires diameters could measure up to 3.5 and 1.8 fold the original pores diameters for membranes respectively with 100 and 200 nm pores diameters. The nanotubes external diameters were up to 2.4 fold wider than the original pores diameter for membranes with a 400 nm pores diameter. Current density does not appear responsible of these nanowires enlargement because the same observations were made whatever the current density (Table 2). So, this could occur because of a widening of the nanowires during electrodeposition, either by a radial growth of the CaP nanostructures (exerting pressure on the membrane such as Schönenberg could explain it with metallic nanowires), by pressures exerted by heated bath [46] or by a thermal expansion of the whole membrane. An other probable reason is the possible H$_2$ bubbles that form at the cathode and dilate pores. The nanowires have a uniform diameter on the totality of the length (Table 2). The aspect ratios (L/D) have ranged from 9 to 71 among the nanowires obtained (Table 2). The most interesting aspect ratio (37-71) was logically obtained for nanowires in the membrane whose pores have the smallest diameter (100 nm) followed by the nanowires obtained in membranes with 200 nm nanopores diameter with an aspect ratio from 21 to 53 and finally the smallest aspect ratio (9-25) was obtained for nanowires synthesized in membranes with 400 nm nanopores diameter (Table 2).

A TEM observation (Figs. 6, 7 and 8) completed the structural study of the nanowires. The presented nanowires were obtained in the two
best conditions of synthesis (pulsed potential at $-1.6 \text{ V}_{\text{AgAgCl}}$ (Fig. 6) and pulsed current density at 120 mA cm$^{-2}$ (Fig. 7)) in a membrane with 200 nm pore diameters. TEM observations confirmed the other analyses; SAED patterns and TEM micrographs showed respectively that CaP nanowires are polycrystalline and constituted by an entanglement of needles oriented along their longitudinal axis (Fig. 6a, V3-60K, b, a, b). TEM micrographs at high magnification obtained at 300 KV showed that the nanoneedles were crystallized because of an identified periodicity of the crystalline planes stacking (Fig. 7V1-500K, V1-400K, V2'-500K). Moreover, the observation of less contrasted zones suggests that the core of nanowires is also crystalline (Fig. 7V3-400K).

We have not distinguished significant differences between the two samples (Figs. 6 and 7). The selected area electron diffraction (SAED) patterns (Figs. 6 d3, d4, 7 d1°, d2) revealed polycrystalline state with the main intense reflexions corresponding to the distances of 0.34 nm and 0.28 nm respectively characteristic of the diffraction by the (0 0 2) and (2 1 1) planes of an apatite-like structure. The periodicity of the stacked crystalline planes measured from Fourier Transform pattern (Fig. 7FT) and TEM micrographs at high magnification (Figs. 6V3-400K, 7V1-500K, V1-400K) is consistent with a HA or CDHA phase and the interplanar spacing along the longitudinal axis of nanowires was measured with a periodicity of 0.34 nm corresponding to the interplanar distance of the (002) planes of HA. These observations confirmed the apatite-like structure of the nanowires and that the growth orientation of nanoneedles (oriented preferentially along the longitudinal axis of nanowires (Figs. 6V3-60K, 7a) corresponds to the $\langle 001 \rangle$ crystalline orientation of HA ($c$-axis) that is the preferential growth orientation of HA 1D nanostructures [67].

This observation is in good accordance with the works done by Ferraz who observed that monocristalline HA nanocrystals synthesis occurs below 60 °C and that above this critical temperature, the synthesis leads to polycrystalline form [70]. Xiao also declared that nanowires synthesized using a template-directed method in porous materials are usually polycrystalline [71]. We can hypothesize that the crystalline nanoneedles constituting the nanowires are formed in the first mechanism of nucleation on the cathode [38] and are the same identified by SEM in the sublayer of needles observed in our thin films. Wang et al. [72] observed two distinct layers in HA electrodeposited films which supported the occurrence of two distinct nucleation mechanisms suggested by Elia et al. [38]. The latter have assumed that deposition starts with a two-dimensional growth (instantaneous mechanism) and changes after a few minutes for a three-dimensional growth (progressive mechanism). In our work, many coatings were composed of two layers of particles distinguishable by their morphology: on the top, microsized spheroids formed by a needles agglomeration [34,53] with a sub-layer of dispersed nanoneedles [53]. Thirsk et al. [73] consider to the contrary that 2D and 3D growths can indifferently be issued from gradual or instantaneous nucleation.

The analyses by TEM micrographs (Fig. 8a, b) and SAED patterns (Fig. 8d3°) of nanostructures produced in membrane with 400 nm pores diameter enabled also to conclude to their polycrystalline and apatitic nature with the entanglement of nanoneedles. The periodicity of the stacked crystalline planes measured in the longitudinal axis of the nanoneedles (Fig. V3-400K) (0.34 nm) corresponded also to the interplanar distance of the (002) planes of HA. To the contrary of nanowires obtained in nanopores of 100 and 200 nm diameters, with membranes of 400 nm nanopores diameter, the nanostructures were constituted by randomly entangled nanoneedles, not oriented along the longitudinal axis of nanowires. We could also better distinguish the nanoneedles inside those structures because of a higher transparency to the electron beam (Fig. 8a, b) compared to the nanowires (Figs. 6a, b, 7a, b) at similar magnification. TEM (Fig. 8a, b) combined to SEM observations (Table 2) of structures more porous than nanowires obtained from nanopores of 100 or 200 nm diameters helped us to conclude that nanotubes were synthesized in membranes with 400 nm nanopores diameter. The possibility to obtain nanotubes was confirmed by many SEM observations (Fig. 5).

Growth in pores is recognized to be more complex that in thin films. Many authors [46,44,74] have highlighted that electrochemical behaviour with formation of nanotubes or nanowires is dependant on many parameters such as current density, electrodeposition duration [68,76], potential waveform, growth rate [44], nanowires size (diameter and aspect ratio [74]). For example, Yoo et al. [75] observed for metal nanostructures and anodized aluminum oxide membranes with weak current density that metal electrodeposited slowly and preferentially on cathode surface producing nanowires by a bottom-up growth phenomena i.e. a layer by layer growth from bottom along the nanopores direction whereas a higher current density was accompanied by a wall-surface growth pattern because the high electric field concentrated at the edge of nanopores and preferential electroplating occured through the surface of nanowires [75]. In an other study in polycarbonate membrane, diffusion coefficient appeared dependant on nanopores size [46] explained by a probable viscosity change of electrolyte inside pores. Hydrodynamics motions of electrolyte are necessarily different under the different nanopores diameters [46]. Martin [76] and Ertant [74] affirmed that a short deposition time could generate nanotubes and a longer time, nanowires. Nanowires growth mechanism was also described by Li et al. [77] as a brick-stacked wirelike growth with bricks stacking along the direction of nanopores from the bottom to the top of membrane.

From our study we can guess and explain the nanopores filling mechanism. Nanopores were never closed on their bottom (Fig. 5a) by the gold covering (whatever 300 nm or 1 μm of gold thickness) which generated a gold ring around nanopores (Fig. 5b). Gold could penetrate and deposit on the first nanometers of nanopores walls as it could be seen on SEM micrographs (Fig. 5b). This gold ring acts as a preferential nucleation site.

H$_2$ bubbles progression inside nanopores that physically pushes CaP material against the nanopores walls [45] could explain why we had found simultaneously nanowires and nanotubes in a same sample (Fig. 5e). But others parameters could also explain the nanotubes formation; an insufficient current density proposed by Hulteen [68] could explain why we observed nanotubes with eventually porous walls in membranes with 100 nm pores diameter (Fig. 5d, f) or 400 nm pores diameter (Fig. 5c). Effectively those nanotubes were obtained in pulsed mode with deposition time 1 s and break time 2 s. Our observations of nanowires with membranes of 100 and 200 nm nanopores diameters and nanotubes with membrane of 400 nm nanopores diameter is consistent with the findings of Ertant, Liu et al. [74,78]. They observed that nanopores with a high aspect ratio (close to 60 in their study) favours the nanowires formation with a layer by layer growth and a smaller aspect ratio (close to 11) favours nanotubes formation with a growth on nanopores walls enabling us to establish the mechanisms of nanopores filling (Fig. 9a, b). Our observations enabled us to suggest that nanoneedles growth in nanowire shape from the bottom to the top of membranes with a preferential orientation parallel to the long-axis of nanopores (Fig. 9b') [77]; in this situation the role of gold ring seems to be major while nanoneedles in nanotube shape seem to nucleate and growth preferentially on the pores walls (probably by adsorption) in a randomly orientation (Fig. 9a').

A gold coating of 300 μm thickness on membranes with 400 nm nanopores diameter leaves on the bottom of nanowires non gold covered area wider than the ones on the bottom of 100 or 200 nm diameter nanopores. This could explain why the gold ring at the bottom of 400 nm diameter nanopores that act as a nucleation site enabled the nanotubes formation instead of nanowires formation. Spain [79] observed a phenomenon corroborating the effect of gold ring; in polycarbonate membrane, metallic nanowires were synthesized when pores were closed by gold on the conductive side whereas nanotubes were synthesized when gold was removed from the bottom of the pores leaving just a gold ring.

In our study, the observation of nanotubes with porous walls
Fig. 9. Hypothesized schematic mechanism of nanotubes (a and a’) and nanowires (b and b’) growth: a and b) (longitudinal) cross sectional view of nanopores; a’ and b’) deposited nanopore wall.

(Table 2 and Fig. 5c, f) and an almost complete length (13.2 μm) after a short time (5 min) that has changed little with doubling time (Table 2) and the observation to the contrary of nanowires from narrower nanopores that were partially filled after 5 min, let us conclude that in this situation, the polycarbonate of nanopores walls have a highly significant role as nucleation sites. The preferential deposition observed along the nanopores walls could be due to an ions adsorption by electrostatic and ionic factors [80] such as the Van der Waals forces. Electrolytic ions could adsorb and preferential nucleation could be due to opposite charges. According to the idea suggested by Tourillon [81], a complexation of Ca\(^{2+}\) cations from calcium salts in electrolytic bath with carbonates functions (-CO\(_3\)\(^{2-}\)) of polycarbonate membrane could be possible and explain the preferential nucleation on nanopores walls. The lines of electrical field may also be different with different nanopores diameters. The gradient of electrolyte concentration that determinates many parameters such as diffusion current is also higher in narrower nanopores enabling to explain a different behaviour with membrane of high and low aspect ratio nanopores [74]. Cao explained a preferential deposition of materials on nanopores walls of a polycarbonate membrane with wider pores by a higher surface area providing more active sites (energetically favourable) for ions adsorption before their reduction [80].

5. Conclusion

Multiplicity of electrochemical deposition parameters had made difficult the obtention of CDHA alone in dense and well-crystallized thin films but we succeeded to determine the optimal conditions for CDHA synthesis on gold substrate. The different analyses carried out (XRD, Raman, FTIR and EDX spectroscopies, SAED, SEM and TEM) were not sufficient to determine the exact nature of the CaP phases. A heat treatment helped us to conclude that compounds in thin films were composed of one only crystalline phase of CDHA. By transferring the best conditions in polycarbonate membranes, we have succeeded for the first time in synthesizing high aspect ratio isolated CDHA nanowires (ranging from 19 to 71) by a template-assisted electrodeposition with a pulsed method in acidic aqueous baths (pH6) composed of 0.042 molL\(^{-1}\) Ca(NO\(_3\))\(_2\) and 0.025 molL\(^{-1}\) NH\(_4\)H\(_2\)PO\(_4\) with the presence of 9% H\(_2\)O\(_2\). Nanowires were obtained with an applied potential of \(\text{-1.6 V/Ag/AgCl}\).

This pioneer method provides an efficient way to synthesize CDHA nanowires and nanotubes. It has the advantages of being a simple, inexpensive, green and fast method representing a high industrial interest. Moreover, it has a great capacity of control onto morphology and size that is missing in others methods of nanostructures synthesis and nanowires in particular. The length, diameter and quantity of the nanowires can be controlled by the characteristics of the chosen membrane (thickness, pores diameter and pore density) but also by deposition duration and current density [44,82]. The size of nanowires diameter controls also the morphology of 1D structures (nanotubes or nanowires) and would have a major role according to Ertan [74]. A TEM analysis highlighted that the produced nanowires and nanotubes were polycrystalline and constituted of nanoneedles with an apatite-like structure. A maximal length close to 16 μm was obtained for nanowires in 5 and 15 min of effective deposition time respectively for membranes with pores diameter 100 and 200 nm and in 10 min for nanotubes in membranes with 400 nm pores diameter. Produced nanowires have the advantage of a high aspect ratio (19-71) with calibrated size and synthesized nanotubes benefit from a high specific surface area [79] which compensates a lower aspect ratio (9-25).

By the same time, this study enabled to understand the mechanism of nanowires filling in polycarbonate membrane with preferential nucleation on gold in membranes with 100 and 200 nm nanopores diameter and growth along the longitudinal axis of nanopores, whereas a preferential and randomly nucleation on nanopores walls in membranes with 400 nm nanopores diameter corroborating the affirmation of Ertan et al. [74].

New processing of CDHA brings new opportunities to study its properties and interactions and consequently to understand its role in mineralized structures. Many studies [9,15] confirmed that nanowires or nanotubes (of HA or CDHA in particular) by a high aspect ratio and a high specific surface area can mechanically and biologically reinforce matrices in bone substitutes but tested 1D nanostructures have generally a wide size distribution and a low aspect ratio.

We can easily affirm that the CDHA calibrated nanowires (or nanotubes) synthesized in this work will optimize the mechanical and biological performances of particles for bone substitutes. Furthermore, the homogeneity of the nanowires that we produced may make us think that the mechanical or biological responses of future experiments will be more reproducible than with less homogeneous 1D nanostructures obtained by other methods. Their use and study will allow a better understanding of size and aspect ratio impacts for those properties and a better understanding of properties and behaviour of the materials at nano-, micro- and macroscopic scales.
Acknowledgments

The authors have a thought for Mr. Patrick Baudart for the preparation of electrochemical cell and little materials used. The authors thank Eric Gautron from the Institut des Matériaux Jean Rouéx IMN (Nantes, France) for his help to the TEM experiments and for access to the TEM facilities of IMN. This work was supported by the Fondation pour la Recherche Médicale, grant number DCM 20111223750 to Chopart.

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